

〔ORIGINAL〕

In vitro mineral induction by immobilized phosphoprotein
—Effect of phosphate group on interfacial tension for mineral induction—

Shuichi ITO, Takashi SAITO, Miles A. CRENSHAW*,
Hiroki TOYOOKA and Koichi MATSUDA

Department of Operative Dentistry and Endodontology, School of Dentistry,
Health Sciences University of Hokkaido

*Dental Research Center, School of Dentistry, University of North Carolina
Biomineralization Laboratory

(Chief : Prof. Koichi MATSUDA)

*(Chief : Prof. Miles A. CRENSHAW)

Abstract

Phosphoproteins are thought to play a primary role in the deposition of mineral on the collagen of dentin. We previously reported that immobilized phosphoproteins reduced activation energy for mineral induction in metastable mineralizing solutions, and that phosphate ester was essential for mineral induction. Interfacial tension is a good measure to evaluate the mineral induction potential because it is a function of the activation energy.

The purpose of this study was to determine the effect of phosphate ester on interfacial tension for mineral nucleation by immobilized phosphoprotein. Phosvitin from egg yolk was used as a model phosphoprotein in this study. Phosvitin was cross-linked to agarose beads with divinyl sulfone. A portion of the cross-linked phosvitin was partially dephosphorylated with potato acid phosphatase. Then, samples were incubated at 37°C in metastable solutions that do not spontaneously precipitate, and the mineral induction time was determined in the samples. The mineral formed was confirmed by X-ray diffraction to be hydroxyapatite. Using classical nucleation theory, the interfacial tension for hydroxyapatite nucleation by intact phosvitin was determined to be 91.3 ergs/cm², it was 93.2 ergs/cm² for 50%-dephosphorylated phosvitin, and 98.1 ergs/cm² for 70%-dephosphorylated phosvitin. Mineral formation was not induced by phosvitin that had been 94%-dephosphorylated. These results indicate that the potential of hydroxyapatite nucleation of phosvitin is high as long as it has a minimum number of phosphate esters for hydroxyapatite nucleation, and that the interfacial tension for hydroxyapatite nucleation by immobilized phosphoprotein is dependent on the degree of phosphorylation.

Key words : Phosphoprotein, Mineral induction, Phosphate group, Interfacial tension.

Introduction

Acidic macromolecules including phosphoglycoproteins, sulfated carbohydrates, acidic proteins, and acidic phospholipids have been associated with biomineralization *in vivo*¹⁻¹²). An understanding of how acidic macromolecules control induction and growth of mineral has potential applications in medicine and biomaterials science. We have been focusing on phosphoproteins which have been considered to have a primary role in nucleation of mineral in dentin⁴⁻⁹). When phosphoproteins are free in solution they inhibit mineral nucleation and crystal growth on apatite from spontaneously precipitating solutions. However, when they are immobilized on insoluble substrates such as agarose beads and collagen fibrils, they induce mineral formation from metastable solutions that do not spontaneously precipitate⁴⁻⁸). It was found that mineral induction time increased with progressive dephosphorylation of immobilized phosphoprotein, and it was concluded that phosphate esters in phosphoprotein are required for mineral nucleation⁴).

We are interested in defining the role of the surface in mineral induction. The interfacial tension for mineral nucleation is a good measure of the mineral induction potential of a surface¹³). We previously reported that interfacial tension for hydroxyapatite nucleation on phosphophoryn was 90.1 ergs/cm²⁻⁵), similar to the interfacial tension (91.0 ergs/cm²) for hydroxyapatite nucleation on hydroxyapatite determined by Christoffersen *et al.*¹³). This led to the assumption that highly phosphorylated surfaces have similar interfacial tension for hydroxyapatite nucleation.

The objective of this study was to determine whether interfacial tension for hydroxyapatite nucleation on immobilized phosphoprotein depends on phosphate ester.

Materials and methods

1. Immobilization of Phosphoprotein to Agarose Beads

Phosvitin (Sigma Chemical Co., St. Louis, MO) was used as a model phosphoprotein in this study. It has a 35 kDa apparent molecular weight, and contains 57% serine + phosphoserine, 9.1% -isoleucine, 6.8% -lysine, and the phosphate content is 24.6% (w/w). Phosvitin was immobilized to agarose beads (Sepharose 4B, Pharmacia Fine Chemicals, Uppsala, Sweden) with divinyl sulfone (Sigma Chemical Co., St. Louis, MO)¹⁵). The amount of phosvitin immobilized to agarose beads was determined by phosphate assay with Malachite Green¹⁶).

2. Dephosphorylation of Immobilized Phosphoprotein

Phosvitin covalently crosslinked to agarose beads was partially dephosphorylated with potato acid phosphatase (Sigma Chemical Co.) in 10 mM Sodium acetate buffer containing 50 μ M EDTA, pH 5.8 at 37°C¹⁷). The amount of remaining organic phosphate ester was

measured in dephosphorylated phosvitin.

3. Mineral Induction Experiment

The compositions of the metastable calcium phosphate solutions that were used in this study are shown in Table 1. The degrees of solution saturations $[\log(\text{ion activity product}) / \log(\text{activity product at saturation})]$ with respect to hydroxyapatite were calculated using computer program WATEQ4F¹⁸⁾. Mineralizing solution saturations of 7.41, 7.53, 7.59 and 7.74 were used. In all cases, the mineralizing solution had a molar Ca/P of 1.67, contained 10 mM Hepes-KOH for buffering at pH 7.40 at 37°C, and 0.02% sodium azide to prevent bacterial growth, and had a final ionic strength adjusted to 0.16 with KCl. The solutions were filtered through a 0.22 μm filter. None of these solutions spontaneously precipitated, even when held at 37°C for seven days.

Table 1 Composition of metastable calcium phosphate solution

[Ca][P] (mM ²)	Ca (mM)	PO ₄ (mM)	KCl (mM)	Hepes (mM)	Saturation
3.30	2.35	1.41	150	10	7.782
3.15	2.29	1.37	150	10	7.650
3.00	2.24	1.34	150	10	7.585
2.70	2.12	1.27	150	10	7.411

Ten microliters of each sample were incubated in 3 ml of the metastable solutions at 37°C in a shaker (ADVANTEC TOYO, TS-200, Tokyo) operated at 125 rpm. Samples were taken at several time points and filtered. The filtrate was dissolved in 0.1N HCl containing 0.25% lanthanum chloride. Then, samples were analyzed for calcium by atomic absorption spectrometry (Perkin-Elmer, Model 5100, Norwalk, Conn, U.S.A.).

The induction time was determined from a plot of Ca (μg) vs. incubation time (sec). Using this information, a slope of the plot of $\log(\text{induction time})$ vs. $(\log \text{saturation})^{-2}$ was identified. The value of this slope was used to calculate the interfacial tension.

4. Interfacial Tension

Mineral nucleators reduce the free energy required for nucleation, then facilitating crystal nucleation from solutions that do not spontaneously precipitate. The interfacial tension between the substrate and the crystalline phase formed is a good measure of the nucleation potential of the substrate¹⁹⁾. The interfacial tension (σ), as described by classical nucleation theory²⁰⁾, was calculated as follows:

$$\sigma = 2.303kT[(5\alpha)/2\beta v^2]^{1/3}$$

σ = interfacial tension

k = Boltzmann's constant (1.38×10^{-6} ergs/deg)

T = temperature in degrees Kelvin (310.15°K)

α = slope of $\log(\text{induction time})$ vs. $(\log \text{saturation})^{-2}$

β = a dimensionless geometric factor ($16\pi/3$ for spherical)

v = molecular volume of hydroxyapatite (2.8×10^{-22})

5. Scanning Electron Microscopy

Mineral formed was collected by filtration onto a $0.2\mu\text{m}$ polycarbonate membrane, rinsed with water adjusted to pH 10 with NH_4OH , coated with gold, and observed in a JEOL JSM-T100.

6. Micro Area X-ray Diffraction

Mineral formed was rinsed with water adjusted to pH 10 with NH_4OH , dried, and identified using RIGAKU RINTO-2000 ($\text{Cu K}\alpha$, 50kV, 25mA).

Results

The phosphate determination showed that the phosvitin covalently crosslinked to agarose beads was $12.2\mu\text{g}/\mu\text{l}$ beads.

Intact and three degrees (49.5%, 71.1% and 94.0%) of dephosphorylated phosvitin were obtained. The intact phosvitin, 50%- and 70%-dephosphorylated phosvitin induced mineral

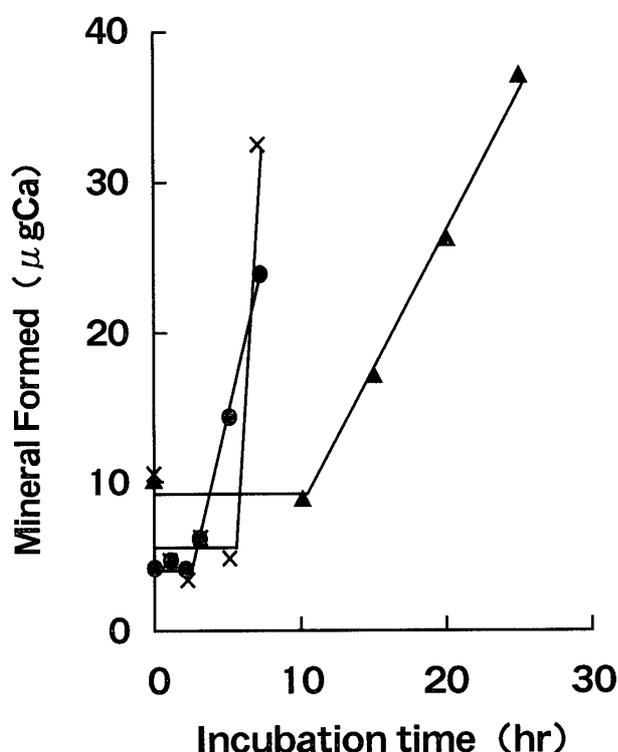


Fig. 1 Mineral induction by intact PV-Agarose beads

Determination of mineral induction times by intact phosvitin cross-linked to agarose beads in metastable solution having the saturation of 7.74 (●), 7.59 (×), or 7.53 (▲).

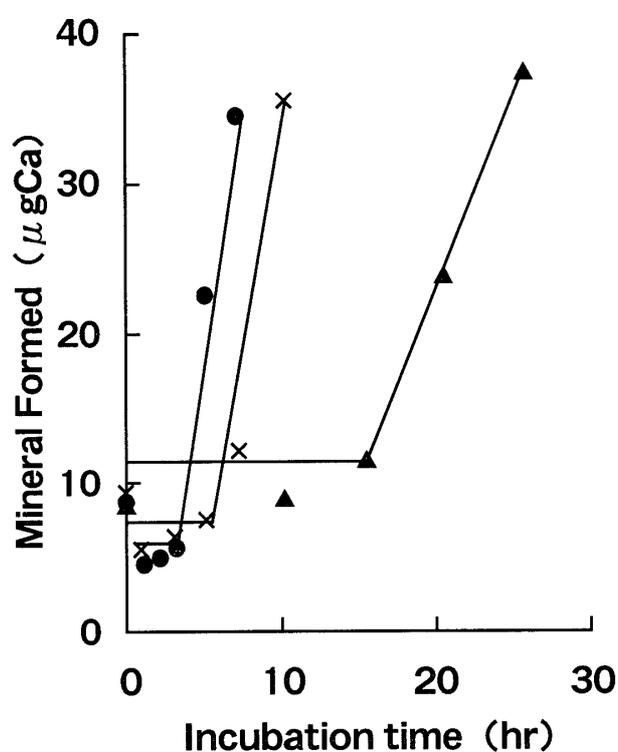


Fig. 2 Mineral induction by 50%-Dep PV-Agarose beads

Determination of mineral induction times by 50%-dephosphorylated Phosvitin cross-linked to agarose beads in metastable solution having the saturation of 7.74 (●), 7.59 (×), or 7.53 (▲).

formation in the mineralizing solution (Figure 1, 2, and 3), while the 94%-dephosphorylated phosvitin did not induce mineral formation. Increasing the solution saturation decreased mineral induction time. Also, mineral induction time increased with progressive dephosphorylation of phosphoprotein.

The interfacial tension for each of these preparations was calculated from the slope of a plot of $\log(\text{induction time})$ vs. $(\log \text{saturation})^{-2}$ (Fig. 4). Interfacial tension for hydroxyapatite nucleation on intact phosvitin was 91.3 ergs/cm², it was 93.2 ergs/cm² for 50%-dephosphorylated phosvitin, and 98.1 ergs/cm² for 70%-dephosphorylated phosvitin (Table 2).

Electron microscopic observations showed that large crystals were formed on the surface of agarose beads in intact, 50%- and 70%-dephosphorylated phosvitin, and that crystals were not formed with the 94%-dephosphorylated phosvitin (Fig. 5).

Micro area X-ray diffraction showed that the crystals formed were all hydroxyapatite (Fig. 6). The peaks were broadened, suggesting carbonate-containing or calcium-deficient hydroxyapatite was formed.

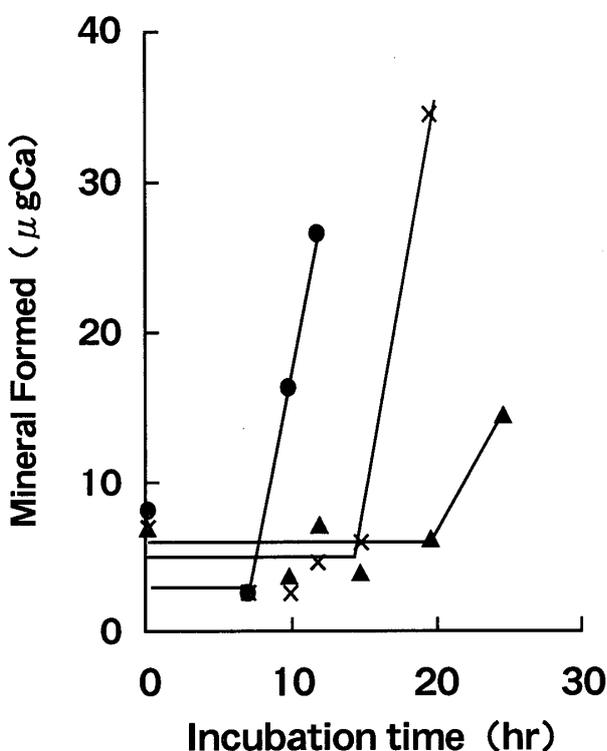


Fig. 3 Mineral induction by 70%-Dep PV-Agarose beads

Determination of mineral induction times by 70%-dephosphorylated Phosvitin cross-linked to agarose beads in metastable solution having the saturation of 7.74 (●), 7.66 (×), or 7.59 (▲).

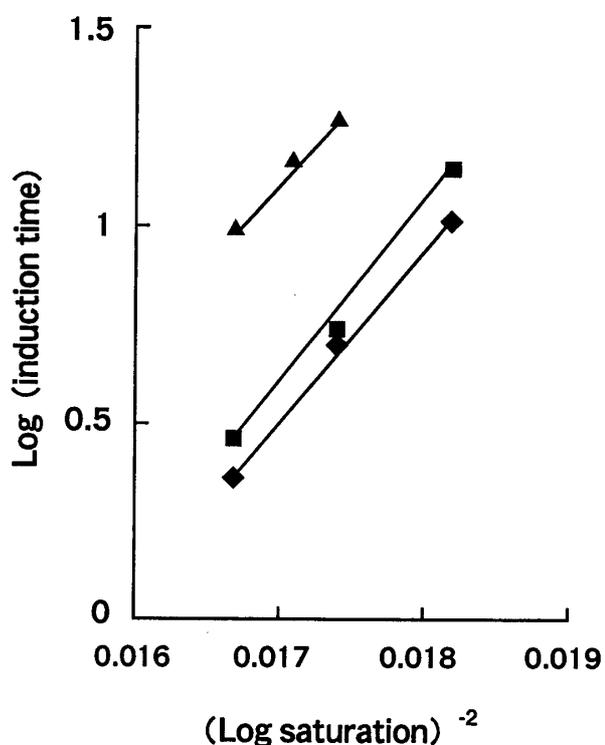


Fig. 4 Plot for determination of the interfacial tension

Plot for determination for interfacial tension. The slopes of the lines for intact phosvitin (◆), 50%-dephosphorylated phosvitin (■), and 70%-dephosphorylated phosvitin (▲) were used to calculate the interfacial tension.

Table 2 Interfacial tension for hydroxyapatite nucleation on phosvitin

	Interfacial Tension (ergs/cm ²)
intact-PV	91.3
50%Dep-PV	93.2
70%Dep-PV	98.1

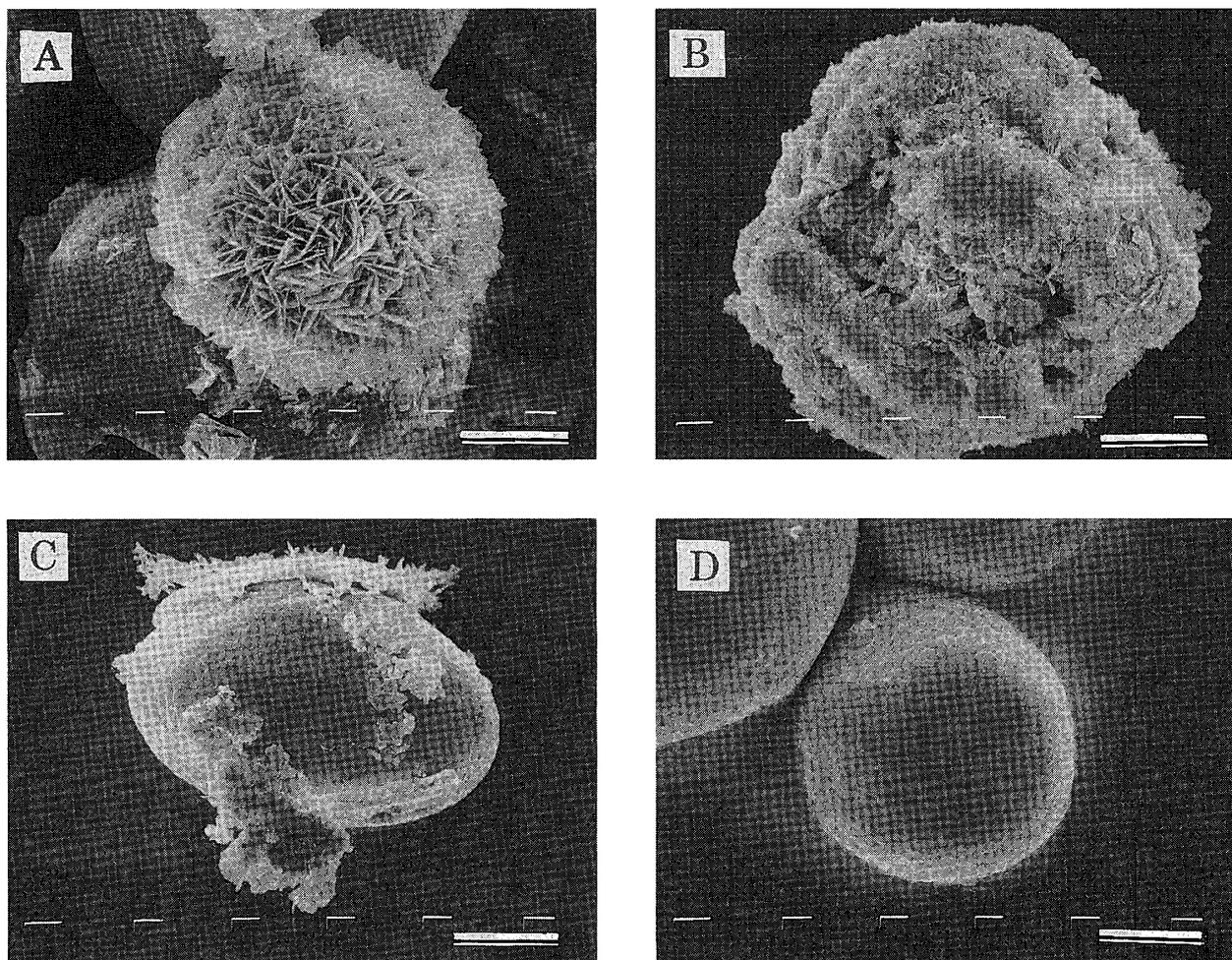


Fig. 5 SEM photographs of mineral formed on phosvitin cross-linked to agarose beads one day after incubation in the solution with saturation 7.59. The crystalline clusters were formed on the surface of agarose beads in (a) intact phosvitin, (b) 50%-dephosphorylated phosvitin, and (c) 70%-dephosphorylated phosvitin, (d) 94%-dephosphorylated phosvitin cross-linked to agarose beads did not induce mineral formation. (Bar = 10 μ m)

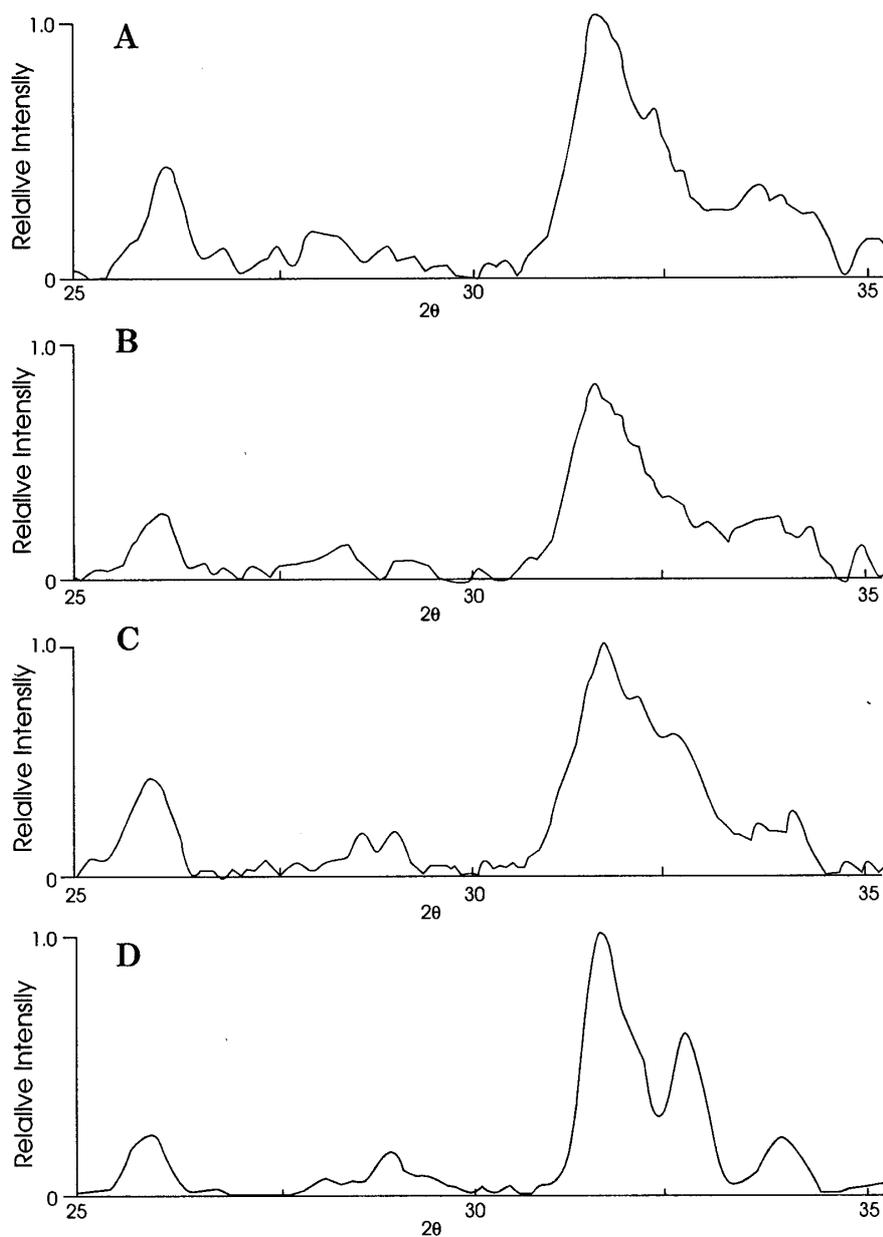


Fig. 6 Micro-area X-ray diffraction pattern of mineral formed by (A) intact phosvitin, (B) 50%-dephosphorylated phosvitin, and (C) 70%-dephosphorylated phosvitin cross-linked to agarose beads, and (D) hydroxyapatite.

Discussion

Previously, we reported that immobilized phosphoproteins induced mineral formation while free phosphoproteins did not induce from metastable calcium phosphate solutions⁴⁻⁹. These findings suggested that immobilized phosphoproteins bind most strongly and in a stereospecific way to calcium phosphate complexes that present a complementary constellation of surface charges. On the other hand, free phosphoproteins self-associate, and this may make the overall free energy of binding to their complementary surfaces decrease.

In the study here, we confirmed that a minimum amount of phosphate ester is required for mineral nucleation in immobilized phosphoprotein. The mineral formed by immobilized phosphoprotein was confirmed as a hydroxyapatite by X-ray diffraction pattern.

Heterogeneous nucleation reduces the activation energy required for crystal nucleation in the solution that does not precipitate spontaneously. The interfacial tension between the substrate and the crystalline phase formed is the most important factor controlling the crystal nucleation process. When the surface of the solid substrate match well with the crystalline phase, interfacial tension becomes very small¹³⁾.

In the present study, increasing the solution saturation decreased mineral induction time with regard to intact, 50%- and 70%-dephosphorylated phosphoprotein. Using the data concerning mineral induction time and the classical nucleation theory²⁰⁾, the interfacial tension for hydroxyapatite nucleation on intact phosphoprotein was determined to be 91.3 ergs/cm². This value is consistent with that that we reported previously⁴⁻⁵⁾. With 50%-dephosphorylated phosphoprotein, it was 93.2 ergs/cm², and it was 98.1 ergs/cm² for 70%-dephosphorylated phosphoprotein. However, hydroxyapatite nucleation was not induced by 94%-dephosphorylated phosphoprotein. The interfacial tension for hydroxyapatite nucleation on hydroxyapatite has been reported as 91.0 ergs/cm², and for fluoroapatite, as 113.0 ergs/cm²⁻¹⁴⁾. Therefore, the interfacial tensions that were obtained in this study were dependent on degree of phosphorylation but still similar to that on hydroxyapatite.

This study indicates that interfacial tension for hydroxyapatite nucleation on phosphoprotein is dependent on the degree of phosphorylation, and that the potential of hydroxyapatite nucleation of dephosphorylated phosphoprotein is still high as long as phosphorylation but has a minimum number of phosphate esters for hydroxyapatite nucleation.

Conclusions

1. Mineral induction times increased with progressive dephosphorylation of phosphoprotein. Mineral formation was not induced by phosphoprotein that was 94%-dephosphorylated. This shows that a minimum number of phosphate esters are required for mineral induction.
2. The interfacial tension for hydroxyapatite nucleation on intact phosphoprotein was determined to be 91.3 ergs/cm². For 50%-dephosphorylated phosphoprotein, it was 93.2 ergs/cm², and it was 98.1 ergs/cm² for 70%-dephosphorylated phosphoprotein. The interfacial tension for hydroxyapatite nucleation by immobilized phosphoprotein is dependent on the degree of phosphorylation.
3. The potential of hydroxyapatite nucleation of phosphoprotein is high as long as phosphoprotein has a minimum number of phosphate esters for hydroxyapatite nucleation.

Acknowledgment

A part of this work was supported by NIDR Grant DE10468 and Grant-in-Aids for Scientific Research in Japan 09771635, 09703045 and 1047048. Parts of this investigation were presented

at the 76 th IADR general session (Nice, France, June 25 1998) and at the 107 th Jpn. Asso. Conserv. Dent. general meeting (Fukuoka, Nov. 7 1997).

References

1. Boskey AL: Mineral-matrix interactions in bone and cartilage, *Clin Orthop*, **281** : 244-274, 1992.
2. Veis A : The role of acidic proteins in biological mineralization. Everett DH and Vincent G. (Eds.), *Ions in Macromolecular and Biological Systems*, Bristol, Sciencetechnia, 259-267, 1978.
3. Butler WT: Dentin matrix proteins and dentinogenesis. *Connect Tissue Res.* **33** : 59-65, 1995.
4. Saito T, Yamauchi M, and Crenshaw MA : Apatite induction by insoluble dentin collagen. *J Bone Mine Res.* **13** : 265-270, 1998.
5. Saito T, Arsenault AL, Yamauchi M, et al. : Mineral induction by immobilized phosphoproteins. *Bone*, **21** : 305-311, 1997.
6. Saito T, Toyooka H, Matsuda K, et al. : In vitro mineral induction by insoluble dentin matrix -Kinetics and Energetics-, *Jpn J Conserv. Dent*, **40** : 1324-1331, 1997.
7. Saito T, Toyooka H, Matsuda K, et al. : In vitro mineral induction by insoluble dentin matrix -A role of phosphate group and carboxyl group on mineral induction-. *Jpn J Conserv Dent*, **40** : 1461-1468, 1997.
8. Saito T, Tooyoka H, Ito S, Crenshaw MA, et al. : In vitro mineral induction by insoluble dentin matrix -Effect of phosphate group on Interfacial energy for mineral induction-. *Jpn J Conserv Dent*, **42** : 323-329, 1999.
9. Lussi A, Crenshaw MA, and Linde A : Induction and inhibition of hydroxyapatite formation by rat dentine phosphoprotein in vitro. *Arch Oral Biol*, **33** : 685-691, 1988.
10. Linde A, Lussi A, and Crenshaw MA : Mineral induction by immobilized polyanionic proteins, *Calcif Tissue Int* **44** : 286-295, 1989.
11. Odutuga AA, Prout RES, and Hoare RJ: Hydroxyapatite precipitation in vitro by lipids extracted from mammalian hard and soft tissues, *Arch Oral Biol*, **20** : 311-316, 1975.
12. Boskey AL: Phospholipids and calcification, In: D.W.L. Hunkins (Ed), *Calcified Tissue*. CRC Press, Boca Raton, Fla., 215-243, 1989.
13. Stumm W: *Chemistry of the Solid-Water Interface*, New York, Wiley, 1992.
14. Christoffersen J, Christoffersen MR, and Johansen T: Some new aspects of surface nucleation applied to the growth and dissolution of fluorapatite and hydroxyapatite. *J Cryst Growth*, **163** : 304-310, 1996.
15. Lihme A, Schafer-Nielsen C, Larsen KP, et al. : Divinylsulphone-activated agarose. Formation of stable and non-leaking affinity matrices by immobilization of immunoglobulins and other proteins, *J Chromatogr*, **376** : 299-305, 1986.
16. Baykov AA, Evtushenko OA, and Aavaeva SM: A malachite green procedure for orthophosphate determination and its use in alkaline phosphatase -based enzyme immunoassay. *Anal Biochem*, **171** : 266-270, 1988.
17. Bingham EW, and Farrell HM Jr. : Removal of phosphate groups from casein with potato acid phosphatase, *Biochim Biophys Acta*, **429** : 448-460, 1976.
18. Ball JW and Nordstrom DK : WATEQ4F Open -File Rep. 3, Menlo Park, US Geol Surv, 1991. 91-118.
19. Mann S: Mineralization in biological systems, *Structure and Bonding*, **54** : 125-174, 1983.
20. Nielsen AE: Nucleation in aqueous solution. Peiser, H.S. Ed. *Crystal Growth*, Oxford, Pergamon, 419-427, 1967.